1	Low-Sound-Level Auditory Processing in Noise-
2	Exposed Adults
3	
4	Emanuele Perugia ^{a,*} , Christopher J. Plack ^{a,b} , Michael A. Stone ^{a,*}
5	^a Manchester Centre for Audiology and Deafness, School of Health Sciences,
6	University of Manchester M13 9PL, UK
7	and
8	Manchester University Hospitals NHS Foundation Trust, Manchester, M13
9	9WL, UK
10	^b Department of Psychology, Lancaster University, Lancaster, LA1 4YF, UK
11	*Corresponding authors:
12	emanuele.perugia@manchester.ac.uk
13	michael.stone@manchester.ac.uk
14	
15	Keywords
16	Sub-clinical hearing damage, Noise exposure, Noise-induced hearing loss,
17	Frequency difference limens, Amplitude modulation depth discrimination

18 Abstract

Early signs of noise-induced hearing damage are difficult to identify, as they are 19 often confounded by factors such as age, audiometric thresholds, or even music 20 experience. Much previous research has focused on deficits observed at high 21 intensity levels. In contrast, the present study was designed to test the 22 hypothesis that noise exposure causes a degradation in low-sound-level auditory 23 processing in humans, as a consequence of dysfunction of the inner hair cell 24 pathway. Frequency difference limens (FDLs) and amplitude modulation depth 25 discrimination (MDD) were measured for five center frequencies (0.75, 1, 3, 4 26 and 6 kHz) at 15 and 25 dB sensation level (SL), as a function of noise exposure, 27age, audiometric hearing loss, and music experience. Forty participants, aged 28 33-75 years, with normal hearing up to 1 kHz and mild-to-moderate hearing loss 29 above 2 kHz, were tested. Participants had varying degrees of self-reported 30 noise exposure, and varied in music experience. FDL worsened as a function of 31 age. Participants with music experience outperformed the non-experienced in 32 both the FDL and MDD tasks. MDD thresholds were significantly better for 33 high-noise-exposed, than for low-noise-exposed, participants at 25 dB SL, 34 particularly at 6 kHz. No effects of age or hearing loss were observed in the 35 MDD. It is possible that the association between MDD thresholds and noise 36 exposure was not causal, but instead was mediated by other factors that were 37 not measured in the study. The association is consistent, qualitatively, with a 38 hypothesized loss of compression due to outer hair cell dysfunction. 39

40 1 Introduction

The body of literature related to cochlear synaptopathy (Kujawa and Liberman, 41 2009), also sometimes described as "hidden hearing loss" (Schaette and 42 McAlpine, 2011), has increased rapidly over recent years (for review see 43 Bramhall et al. 2019; Le Prell, 2019; Liberman & Kujawa, 2017; Plack et al. 44 2016). Experimental animal studies have shown that the synapses between 45 inner hair cells (IHCs) and auditory nerve fibers can be damaged permanently 46 as a consequence of either noise exposure or aging, without substantial effects 47 48 on absolute threshold sensitivity (Liberman & Kujawa, 2017; Sergeyenko et al., 2013). Low-spontaneous-rate (SR) fibers may be preferentially affected 49 (Furman et al. 2013; Kobel et al. 2017). Since the low-SR fibers typically have 50 high thresholds and high saturation levels, they are thought to be responsible 51 for coding supra-threshold sounds. Using both psychophysical and 52 electrophysiological measures, noise-induced cochlear synaptopathy has been 53 investigated indirectly in human participants with clinically normal audiograms, 54 with some studies finding evidence for synaptopathy but others not (Bharadwaj 55 et al. 2015; Bramhall et al. 2017, 2019; Couth et al. 2020; Grinn et al. 2017; 56 Grose et al. 2017, 2019; Guest et al. 2017; Liberman et al. 2016; Marmel et al., 57 2020; Prendergast et al. 2017a, 2017b). 58

However, the early effects of noise damage may extend beyond synaptopathy for
low-SR fibers. For the noise-induced cochlear synaptopathy, beside the loss of
low-SR fibers, computational models suggest that a substantial loss of high-SR
fibers is also required to obtain a large perceptual effect (Encina-Llamas et al.,
2019; Marmel et al., 2015; Verhulst et al., 2018). Valero et al. (2017) showed

64 that permanent threshold shifts in macaques after noise exposures up to 146 dB SPL were due to loss of both low- and high-SR fibers. Cochlear synaptopathy is 65 66 commonly understood as primarily affecting low-spontaneous rate fibers, which 67 have high thresholds (Furman et al. 2013). As a consequence of this, the 68 perceptual impact is predicted to be observable at high intensity levels. Evidence for noise-induced low-SR synaptopathy is weak, but modelling suggests a need 69 to explore also the contribution of damage to high-SR fibers (Encina-Llamas et 70 al., 2019; Marmel et al., 2015; Verhulst et al., 2018). Few studies have explored 71 the relation between noise exposure and auditory processing related to loss of 72 73 high-SR fibers (requiring testing at low sensation levels, SLs), which may reflect a different type of sub-clinical hearing damage from that observed with low-SR 74 fibers. Testing at low SLs allows investigation of localized regions of the cochlea, 75 due to less spread of excitation, and therefore stimulation of a more limited 76 number of IHCs. 77

Stone et al. (2008) assessed the listeners' ability to discriminate narrowband 78 sounds with different envelope statistics as a function of low SLs in both a noise-79 80 exposed group and a control group. The sounds were noise bursts with either 81 Gaussian amplitude or "low-noise" statistics (LNN; Pumplin, 1985) centered on 2, 3, or 4 kHz. The LNN was the target sound, which possessed the same power 82 83 spectrum, but lower envelope fluctuations than the Gaussian-statistic noise. 84 Rock musicians and frequent nightclub attendees formed the noise-exposed group (with noisy activities regularly exceeding 100 dBA). Compared to the 85 control group, they had similar absolute thresholds between 2 and 4 kHz (the 86 typical spectral region for noise-induced hearing damage, Smoorenburg, 1992) 87

88	but were, on average, younger (22 vs. 29 years). Performance was measured as
89	the duration of a signal burst (in ms) required in order to discriminate between
90	the two noises, with longer times indicating worse performance. As the
91	presentation level decreased to 12 dB SL, the performance of the noise-exposed
92	group worsened, showing poorer fidelity of envelope coding. The results were
93	interpreted as subtle IHC damage due to the long-term noise exposure.
94	However, at least three out of 10 control subjects showed performance similar to
95	that of the noise-exposed group at some frequencies.
96	The use of personal music players (PMPs), such as MP3 players or smartphones,
97	is one particular ubiquitous cause of noise exposure (Le Prell et al. 2013;
98	Sulaiman et al. 2014; Kumar et al. 2017). Some effects of PMP exposure were
99	investigated by Vinay & Moore (2010) in 14 male participants using two
100	psychophysical tasks: frequency difference limens (FDLs) at 20 dB SL, and
101	amplitude modulation detection (AMD) at 10 and 20 dB SL. Eight of the
102	participants were habitual PMP users while the remaining six were not. The
103	experimental group was again, on average, younger than the control group (27.6
104	vs. 33.6 years). In the frequency range from 3 to 8 kHz, the experimental group
105	had lower absolute audiometric thresholds (3-5 dB) and higher (worse)
106	thresholds in the frequency discrimination task. Interestingly, the reverse was
107	true for the AMD task, as the experimental group showed lower (better) AMD
108	thresholds at 4 and 6 kHz relative to the control group. The authors suggested
109	that this reflected mild outer hair cell (OHC) dysfunction producing loudness
110	recruitment and potential magnification of amplitude modulation (AM)
111	fluctuations (Moore et al. 1996).

112 The contribution of possible IHC and OHC dysfunction due to noise exposure and/or aging, and its effect on AMD, was further evaluated by Stone & Moore 113 114 (2014). The cross-sectional study involved young (18-24 years) and older (26-35 years) participant groups, and each group was subdivided into low- and high-115 noise exposure subgroups with 16 participants in each subgroup. The AMD task 116 was measured for carrier frequencies of 3, 4 and 6 kHz and at 10, 25 and 40 dB 117 SL, using a modulation frequency of 25 Hz. Although there were some 118 differences in pure-tone hearing thresholds among the subgroups, all 119 participants had thresholds in the range of normal to mild. As the authors 120 121 pointed out, the results for the AMD task at 10 dB SL were "somewhat paradoxical" because the high noise-exposure groups had higher (worse) AMD 122 thresholds than the low-noise groups, but the older group, which had worse 123 absolute thresholds and greater noise exposure, showed better AMD thresholds 124 125 than the young group. Since the pattern of results cannot be ascribed only to a loss of either IHC or OHC function, they were explained as a balance between 126 IHC and OHC dysfunction that may depend on different combinations of 127 128 intensity, duration and regularity of noise exposure.

The above-mentioned studies employing low SLs attempted to detect early signs of noise-induced hearing damage. The diverging results may be due to one or some of the following reasons: First, poor quantification of noise exposure. In the present study we used the retrospective self-report interview developed in our laboratory, the "noise exposure structured interview" (NESI; Guest et al. 2018), which was effective in tinnitus classification (Guest et al. 2017) and has been shown to correlate with a measure of noise-induced cochlear synaptopathy

(Shehorn et al., 2020). Second, in studies with a small number of participants, 136 the psychophysical tasks may have lacked sensitivity because the between-137 138 subject variability was large (Hedge et al. 2018; Heinrich & Knight, 2020). Third, previous work mostly focused on young adults with normal audiograms, 139 neglecting the possible effects of age on hearing damage; measures of deficits 140 accrued through prolonged noise exposure may be required (see also Carcagno 141 & Plack, 2020; Prendergast et al. 2019; Valderrama et al. 2018). Here we tested 142 a cohort of adults aged 33 to 75 years with mean pure-tone hearing thresholds 143 in the range of normal to mild loss. The selection criteria were intended to 144 145 disentangle the effects of age, hearing threshold and noise exposure on IHC and 146 OHC dysfunction. Participants with normal hearing should have mainly IHC damage due to noise exposure (Bramhall et al., 2017), whereas participants with 147 mild hearing loss may have damage to both IHCs and OHCs (Johannesen et al., 148 149 2014). Fourth, despite the fact that music experience may improve performance on psychoacoustic tasks (Yeend et al., 2017), confounding the effects of noise 150 exposure (see also Couth et al., 2020), it was not accounted for in previous low-151 SL studies. Indeed, the majority of noise-exposed participants in Stone et al. 152 (2008) were also musicians. Here we included participants with a range of 153 music experience, including expert musicians. The current study therefore 154 aimed to control better for these possible confounds. 155

156 This study was in the framework of a larger study (Stone et al. submitted) that

157 aimed to evaluate the Threshold Equalizing Noise (TEN) test (Moore et al.

158 2004) as a possible early clinical indicator of damage to cochlear structures

159 other than OHCs. The hypothesis was that noise-induced cochlear damage

160 would affect high-SR fibers; hence the perceptual consequences would be 161 measurable at low SLs. In adults with hearing level ranging from normal to 162 mild, we predicted impaired frequency discrimination and AM depth discrimination (MDD) at low SLs in those with high noise exposure compared to 163 those with low noise exposure. Although some authors have suggested that the 164 effects may be too small to measure perceptually (e.g., Oxenham, 2016), 165 166 previous work has provided evidence for a relation between noise exposure and performance on FDLs and AMD thresholds (Vinay & Moore, 2010; Stone & 167 168 Moore, 2014), suggesting that behavioral measures may be sensitive to high-SR 169 dysfunction.

170 2 Methods

171 2.1 Participants

Forty participants (20 females) between the ages of 33 and 75 years (mean 58.7 172 years) were selected from a larger pool of participants (N=112) recruited for an 173 experiment to be reported elsewhere (Stone et al. submitted). The selection 174 criteria for the sub-group were that they had, in the test ear, normal pure-tone 175 176 hearing thresholds up to 1 kHz (i.e., average of 0.5, 0.75 and 1 kHz \leq 20 dB HL) and a mild-to-moderate threshold between 3 and 6 kHz (i.e., average of 3, 4 and 177 6 kHz > 20 dB HL). Participants with asymmetrical hearing loss, whether 178 sensorineural or conductive in origin, were tested in their better ear only, and 179 180 efforts were made to exclude conductive losses with average air-bone gap at 0.5, 181 1 and 2 kHz of greater than 10 dB.

182 The study was approved by the National Research Ethics Service (NRES)

184 REC number 16/NW/0260) and all participants gave informed consent.

185 **2.2 Pure tone audiometry**

186 Air-conduction and Bone-conduction audiometry were performed for each 187 individual ear in accordance with British Society of Audiology's recommended 188 procedure (British Society of Audiology, 2018). Air-conduction audiometric thresholds (Fig. 1) were measured at 11 frequencies between 125 Hz and 8000 189 Hz (i.e., octave frequencies from 125 Hz to 8000 Hz, and the half-octaves of 190 191 750, 1500, 3000 and 6000 Hz) using a Madsen Astera2 and TDH-39 supraaural headphones. Bone-conduction audiometric thresholds were measured at 192 500, 1000, 2000, and 4000 Hz using a Radioear B71 bone vibrator. 193

194 2.3 Noise exposure

Lifetime noise exposure was estimated using the NESI (Guest et al. 2018). 195 During this interview, participants identified noisy activities (such as 196 recreational, occupational or educational, and firearm impulse exposures) to 197 198 which they had been exposed, the duration of exposure to each activity (number of hours per day, days per week, weeks per year, and years), and hearing 199 protection use in these activities (if any). The sound levels of these activities 200 were estimated by the participants based on the vocal effort required to hold a 201 conversation. For instance, if a participant thought that conversation required 202 shouting at a listener 4 feet (1.2 m) away, then the level was recorded as 99 dBA. 203

204 2.4 Music Experience

205 The NESI was also used to construct a proxy measure of a participants' music

206 experience. In particular, the total number of hours of playing a music instrument and/or singing (e.g., in front of an audience) was taken as the metric 207 208 of music experience. The metric cannot discriminate participants with formal and informal (e.g., self-taught) music training, or those who either played, or 209 used to play, at the time of the research, and the regularity of instrument 210 playing. However, this metric was used previously (Prendergast et al., 2017b) 211 and approximates the "Index of Music Instrument Playing" of the Music Use 212 Questionnaire (Chin & Rickard, 2012). 213

214 2.5 Psychophysical tasks

215 2.5.1 General procedure

All testing was performed in a double-walled sound-attenuating booth in two 216 separate sessions. Monaural stimuli were generated (24-bit resolution, 44.1 kHz 217 218 sampling rate) using the AFC (alternative forced choice) software (Ewert, 2013) in MATLAB (R2015b, 8.6.267246, 64-bit), and presented via a Focusrite 219 Scarlett 2i2 USB sound-card and Etymotic Research ER4s insert earphones. 220 Psychophysical measures of absolute threshold (ABS), taken by the software, 221 were followed by measures of FDLs and AM depth discrimination (MDD). The 222 experiments were performed at five center frequencies (0.75, 1, 3, 4 and 6 kHz), 223 at both 15 and 25 dB SL relative to the ABS. The rationale for the choice of 224 frequencies was that performance at 0.75 and 1 kHz should be less affected by 225 226 noise exposure than would performance at the three higher frequencies (Lutman et al. 2016), therefore controlling better for between-participant 227 variability. The two SLs were chosen because previous studies (Stone & Moore, 228 2014; Vinay & Moore, 2010) had shown a significant difference in performance 229

across low SLs.

The testing order was pseudo-randomized both by frequency, and by SL. All 231 participants were trained in each task until their performance appeared to be 232 stable (e.g., a low standard deviation). Practice runs were performed at a center 233 frequency of 1.5 kHz because this was not used in the experimental tasks. The 234 235 training generally took 1-5 minutes per task. For the data collection, at least two 236 runs were obtained for each frequency and SL. If the standard deviation of the measured variable across reversals was greater than 3 dB, or if the difference in 237 threshold between runs exceeded 5 dB, an additional run was obtained. The 238 239 final thresholds were based on the average over runs. Visual feedback was provided indicating correctness of the response. In order to limit the possible 240 variation of the intended presentation level within any frequency, the 241 242 participants were instructed not to move or touch the insert earphones until all the measures for that frequency were taken. The participants were offered a rest 243 break once all of the measures for a single frequency were collected. 244

245 2

2.5.2 Absolute Threshold

For each test frequency, ABS was measured for pure-tone signals in quiet using 246 247 a three-alternative forced-choice method, with a two-down, one-up, adaptive tracking procedure. One random interval contained a pure tone whereas the 248 others had no sound. The step size was initially 6 dB until the first reversal, 249 250 decreased to 4 dB until the next reversal, and then was kept at 2 dB for six reversals. The threshold was estimated as the mean level of the last six reversals. 251 The signals lasted 300 ms, including 10 ms ramps, with a 400 ms inter-stimulus 252 interval. 253

254 2.5.3 Frequency Difference Limens

A two-alternative forced-choice paradigm, with a two-down one-up adaptive 255 tracking procedure, was used. One interval contained four identical tone bursts 256 257 (AAAA), while the other interval contained two alternated (target) bursts with a Δf ratio change in frequency between them (A'B'A'B'). The FDL was measured 258 with the alternated bursts having symmetric shifts (on a log-frequency scale) 259 around the test frequency. Tone burst duration was 400 ms including 20 ms 260 261 ramps; the within-interval gap between each tone was 90 ms and, across-262 intervals, 400 ms. In order to reduce the availability of loudness cues, the level 263 between individual bursts was randomly roved by $\pm 3 \text{ dB}$, quantized in 1-dB 264 steps. The frequency ratio was calculated as:

265
$$\Delta f = (1 + 10^{(0.1 * \Delta f_n)})$$

where Δf_n was varied in dB. The step size was 10 dB until the first reversal, decreased to 5 dB until the next reversal, and was then 2 dB thereafter for six reversals. The participant's task was to indicate the interval containing the bursts alternating in frequency. The value of Δf was decreased following two correct responses in a row or increased following one incorrect response. The mean Δf was calculated as the geometric mean of the last six reversals.

272 2.5.4 Amplitude Modulation Depth Discrimination

A two-alternative forced-choice paradigm was used to measure the threshold for discriminating modulation depth. One interval contained the standard (target) AM tone with a modulation depth (m_s) fixed at 50% (i.e., -6 dB), while the other interval contained the comparison AM tone with a modulation depth (m_c)

initially set at 10% (i.e., -20 dB, a very shallow modulation). The depth in the 277comparison interval was always less than the standard depth. The tones had a 278 279 modulation rate of 15 Hz, were 340 ms in duration, including 20 ms ramps, and 280 the two intervals separated by a 90 ms gap. The use of an AM-rate of 15 Hz 281 resulted in a narrow-bandwidth signal that fell within the passbands of the 282 auditory filters. A ±3-dB level roving, again with a uniform distribution in 1-dB steps, was applied on each tone to limit overall loudness cues due to differences 283 in modulation depth (Stellmack et al., 2006). The rove range was limited to ± 3 284 dB because of the low presentation levels (15 and 25 dB SL) used in both tasks, 285 286 and because, in the case of the MDD task, the reference modulation range was 287 ± 5 dB. The range chosen ensured that all signals did not drop below audibility, and that the range of signal levels requiring coding did not majorly overlap 288 289 between the two nominal testing levels.

The task was to indicate the interval having the greater modulation depth. 290 Following two correct responses in a row, the modulation depth m_c was 291 increased, while following one incorrect response it was decreased. The 292 modulation depth was varied arithmetically on a logarithmic scale. The initial 293 step size was 4 dB (i.e., 5.8%) until the first reversal, decreased to 2 dB (i.e., 294 2.6%) until the next reversal, and was then 1 dB (i.e., 1.2%) thereafter for six 295 296 reversals. There are several measures for expressing the MDD threshold reported in the literature; here we used the difference in modulation depth 297 between the standard and the comparison (similar to Stellmack et al., 2006), 298 299 both expressed as a peak-to-valley ratio (Moore et al., 1996):

300
$$\Delta m = 20 \log_{10} \left(\frac{1 + m_s}{1 - m_s} \right) - 20 \log_{10} \left(\frac{1 + m_c}{1 - m_c} \right)$$

301 2.6 Data analysis

The Spearman's correlation coefficient was calculated for the NESI score on Age 302 303 because noise exposure and aging are strong and competitive factors as both can produce the loss of IHCs and OHCs. Previous studies were based on group 304 analyses to investigate low SL hearing deficits (Stone et al. 2008; Stone & 305 Moore, 2014; Vinay & Moore, 2010). So as to be able to compare our results 306 with the literature, a similar approach was used via mixed-effects models 307 (Baayen et al. 2008; Winter, 2013). Only participants with low and high noise 308 exposure were included in the modelling. The separation may increase the 309 310 likelihood of observing the effects of noise exposure as a difference between groups if there are floor or ceiling effects (see Prendergast et al., 2017a, 2017b). 311 In order to account for individual differences across participants, the entire 312 cohort was used when calculating the Spearman's correlation coefficient for 313 ranked data (rho). 314

Mixed models were calculated separately for the FDLs and MDD thresholds. In 315 the models, the thresholds were entered as the dependent variable. Age (as a 316 scaled continuous variable), (test) Frequency, SL, Hearing Status group, Noise 317 *Exposure* group, and *Music Experience* groups were evaluated as fixed effects. 318 Random-effects and then fixed-effects were chosen via the backwards selection 319 approach, i.e., a complex and large model was simplified based on step-wise 320 321 deletion of model terms with high p-values (Baayen et al. 2008; Kuznetsova et al. 2015). The models were assessed using the Akaike Information Criterion 322

(Burnham & Anderson, 2002), and the marginal and conditional R². The
marginal R² is the proportion of the variance in the response variable (i.e.,
thresholds) explained by the fixed effects, while the conditional R² is the
proportion of the variance explained by the entire model, including both the
fixed and the random effects (Johnson, 2014; Nakagawa et al. 2017; Nakagawa
& Schielzeth, 2013).

Correlation analyses were performed separately for FDL and MDD thresholds 329 for each combination of frequency and SL. The relation between psychophysical 330 thresholds, NESI and Age was investigated using Spearman's correlation. The 331 relation between psychophysical threshold and NESI was also controlled 332 separately for each of music experience, Age and ABS via partial Spearman 333 correlation. All statistical analyses were performed in R (version 3.6.3, R Core 334 Team, 2020). The mixed models were fitted and evaluated using the packages 335 *lme4* (Bates et al. 2015), *lmerTest* (Kuznetsova et al. 2017) and *performance* 336 (Lüdecke et al. 2020). Post hoc pairwise comparisons were conducted via the 337 estimated marginal means using emmeans (Lenth, 2020) with Kenward-Roger 338 approximation for degrees of freedom and Bonferroni correction for multiple 339 comparisons. Data were visualized within *gaplot2* (Wickham, 2009) using 340 Raincloud (Allen et al. 2019). 341

342 **3 Results**

343 **3.1 Hearing Status, Noise Exposure and Music Experience groups**

344 Participants were divided in groups according to their AC hearing thresholds,

345 NESI score and music experience. Since all participants had normal, or near-

346 normal, hearing thresholds up to 1 kHz, and hearing loss at high frequency, combined low (0.5, 0.75 and 1 kHz) and high (3, 4 and 6 kHz) frequency 347 348 descriptors were used (Fig. 2, panel a). Participants were classified either as Normal/Mild (27 participants, 12 females) with average of ≤20 dB HL at low 349 frequency and between 20 and 40 dB HL at high frequency, or 350 Normal/Moderate (13 participants, eight females) with an average of ≤ 20 dB 351 HL at low frequency and an average of >40 dB HL at high frequency. There was 352 no significant difference between the groups in age [t(38) = -1.688, p = 0.1], 353 NESI score [t(38) = 0.527, p = 0.601] or music experience [W(38) = 126, p = 0.601]354

355 0.126].

The cumulative units of noise exposure (NESI score), *log10* transformed so as to 356 obtain an approximately Gaussian distribution, was used to categorize 357 358 participants into Low, Medium or High Noise-exposure groups (40-20-40% of distribution, respectively, Fig. 2, panel b). The Low and High Noise-exposure 359 groups used in the mixed-effects modelling had median NESI scores of 1.046 360 (range: 0.232-1.510) and 2.233 (range: 1.851-3.203), respectively. However, the 361 362 High Noise-exposure group was significantly younger than the Low Noiseexposure group [t(30) = 3.083, p = 0.004] with median ages of 53 and 64 years, 363 respectively. There was no significant difference between the noise exposure 364 groups in their average PTA [t(30) = 0.619, p = 0.541], or in their music 365 366 experience [W(30) = 101.5, *p* = 0.295].

367 Twenty-one participants (10 females) had no music experience, while 19 (nine
368 females) had either some experience or were expert musicians (Fig. 2, panel c).
369 Groups of listeners with and without music experience did not differ in their age

[t(38) = -0.254, p = 0.801] with median ages of 61 and 59 years, respectively;

nor in their PTA [t(38) = 1.071, p = 0.291], with median values of 22 and 20 dB

HL, respectively; nor in their NESI score [t(38) = 1.343, p = 0.187] with median

373 values of 1.690 and 1.778, expressed as *log10*(*NESI*), respectively.

374 **3.2 Noise exposure**

- 375 Estimated lifetime noise exposure ranged from to 0.232 to 3.203 in *log10* NESI
- units. Our maximum is larger than previously reported (e.g., Prendergast et al.,
- 377 2017b, 2019). This was due to one participant with extensive orchestral
- 378 experience. The other participants' data were within the range of previously
- 379 reported data. There was no difference in the NESI score between females and

380 males [t(38) = -1.282, p = 0.207], with medians (and ranges) of 1.552 (0.232-

- 381 3.203) and 1.770 (0.677-2.690), respectively. There was a negative relation
- 382 between lifetime noise exposure and age (Fig. 3, Spearman's correlation

383 coefficient r = -0.437, p = 0.005).

384 3.3 Psychophysical tasks

385 The results for the psychophysical tasks are shown in Fig. 4 separated by Noiseexposure groups, and in the Supplementary Material, Fig. S1 separated by 386 Hearing Status group, and Fig. S2 separated by the Music Experience group. 387 388 Each figure shows ABS, FDLs and MDD, at 15 and 25 dB SL, as separate panels with a raincloud plot per group. Raincloud plots show mean and standard error 389 (SE) of the thresholds as error-bars, participants' individual data (with some 390 horizontal jitter for clarity) as dots, and probability densities as a 'half violin' 391 plot. The color code is the same as used in Fig. 2 and is included in each ABS 392

393 panel. Table. 1 shows Spearman correlations between the Noise-exposure scores394 and the thresholds for each task.

395 3.3.1 Frequency Difference Limens

- 396 The FDLs were fitted with a mixed model (marginal $R^2 = 0.45$, conditional $R^2 =$
- 397 0.76) having Frequency, Age (scaled), and Music Experience group as fixed
- 398 effects (without the interaction terms); and including by-participant random
- 399 intercepts and by-participant random slopes for Frequency (assuming
- 400 homoskedasticity). FDLs increased (i.e., performance got worse) as a function of
- 401 Age (see Fig. S3). The FDLs were significantly worse at 4 and 6 kHz when
- 402 compared to the lower frequencies. Participants without music experience had
- 403 worse performance [$\Delta f = -0.02 \log 10(\%)$] relative to the participants with music

404 experience [$\Delta f = -0.19 \log 10(\%)$; t(28.8) = 3.954, p < 0.001].

405 3.3.2 Amplitude Modulation Depth Discrimination

406 The specifications of the mixed model (marginal $R^2 = 0.23$, conditional $R^2 =$ 407 0.47) for the MDD thresholds had SL, Noise groups and their interaction, and

408 Music groups as fixed effects; participants were treated as random intercepts. It

is important to highlight that there was no interaction between Noise Exposure

- 410 and Music Experience groupings as the effect of noise exposure was not
- 411 mediated by the effect of music experience. Overall, performance was better
- 412 (lower thresholds) at 25 dB SL (median $\Delta m = 2.13$ dB) compared to at 15 dB SL
- 413 $(\Delta m = 2.44 \text{ dB})$. The High Noise Exposure showed significantly lower MDD
- thresholds than the Low-Noise Exposure group at 25 dB SL [$\Delta m = 1.74$ vs. 2.65
- 415 dB; t(40.4) = -3.36, p = 0.002] but not at 15 dB SL. Furthermore, MDD
- 416 threshold was better for participants with some music experience ($\Delta m = 1.91$

- 417 dB) than for those without $[\Delta m = 2.63 \text{ dB}; t(29.1) = -3.66, p = 0.001]$. There was
- 418 no effect of Hearing Status group: Normal/Mild hearing participants had
- 419 median $\Delta m = 2.33$ dB whereas participants in the Normal/Moderate hearing
- 420 group had median $\Delta m = 2.13$ dB.
- 421 At 25 dB SL, a negative correlation existed between NESI score and MDD
- 422 threshold at 0.75, 3, 4, 6 kHz (Table 1). The effect at 6 kHz was the most robust
- 423 (r = -0.591, p < 0.001) and remained significant even after controlling for Age,
- 424 Music Experience, and ABS; and correcting for multiple comparisons ($\alpha =$
- 425 0.05/100, Bonferroni).
- 426 3.3.3 Exploratory analysis
- Fig. 5 shows the results for the MDD task at 25 dB SL averaged over frequency 427 in terms of the interaction between the Noise Exposure (i.e., Low vs High) and 428 Music Experience (i.e., With vs Without) groups. The differences in the 429 430 thresholds among these four subgroups were evaluated. The thresholds were highest (worst) in the participants with low lifetime noise exposure and without 431 music experience (median $\Delta m = 3.11$ dB). The difference between these and 432 those of the participants with music experience and high lifetime noise exposure 433 $(\Delta m = 1.63 \text{ dB})$ were significant after controlling for six comparisons [W = 0, p] 434 < 0.001]. 435
- 436 4 Discussion

FDL and MDD tasks were used to test the hypothesis that noise exposure is
associated with sub-clinical hearing deficits manifesting at a low SL in adults
with normal hearing to mild hearing loss. The results do not support the

primary hypothesis. In particular, participants with higher noise exposure had
better MDD performance at 25 dB SL. In addition, FDLs did not vary with noise
exposure but improved strongly with music experience and worsened with age.

443 **4.1 Frequency Difference Limens**

The FDLs were dependent on the test frequency and participants' music
experience. FDLs increased (worsened) as a function of increasing frequency,
irrespective of Noise Exposure or Hearing Status groups. The dependence of
FDLs on frequency is well known in the literature. Using data from several
studies, Micheyl et al. (2012) showed that the log-transformed FDL (as in this
study) is well described by a power function of frequency with an exponent of
0.8.

Participants with music experience outperformed other participants. The effects 451 of music experience on the FDLs are consistent with previous studies (Kishon-452 Rabin et al. 2001; Micheyl et al. 2006; Prendergast et al. 2017b). FDLs got 453 worse as function of age as previously reported (e.g., Moore & Peters, 1992). 454 Interestingly, we did not observe any effects of Hearing Status group on the 455 FDLs. Similar observations were reported in a study of complex-tone Fo 456 discrimination. Bianchi et al. (2019) observed similar performance between 457 participants (\geq 55 years old) with and without hearing loss, but improved 458 performance in musicians relative to non-musicians. 459

461 effects or correlation related to lifetime noise exposure in the present study, may

The possible confound due to the music experience and the lack of significant

suggest that the FDL is not a sensitive marker for noise-damage assessment.

20

460

463 Vinay & Moore (2010) reported an association between the use of PMPs and

464 poor FDLs for frequencies centered between 3 and 8 kHz. However, since they

did not record participants' music experience, it is not clear whether music

466 experience could have been a determining factor in their study.

467 4.2 Amplitude Modulation Depth Discrimination

468 In general, a MDD threshold is measured as a function of the AM depth of a

469 standard modulation m_s by varying the modulation depth of a comparison m_c

470 (Ewert & Dau, 2004; Wakefield & Viemeister, 1990). Expressed as

471 $[10log_{10}(m_c^2 - m_s^2)]$, The discrimination thresholds in these studies were around

472 -10 dB, with m_s near to -6 dB (as in the current study). Our grand mean MDD

473 threshold was $\Delta m = 2.6$ dB or, expressed in similar fashion to Ewert & Dau

474 (2004) and Wakefield & Viemeister (1990), -9.4 dB.

475 To the authors' knowledge, MDD thresholds have never previously been

476 measured in studies related to noise-induced hearing loss. Instead, AMD

477 thresholds have been measured more extensively than MDD thresholds. Since

478 the modulation depth $m_s = 0$ dB in the AMD task, the latter can be seen as a

479 special case of MDD. Therefore, the results of our MDD thresholds can be

480 interpreted alongside to those of AMD thresholds.

481 There was no effect of carrier frequency on MDD thresholds (similar to Lee,

482 1994), but performance improved at 25 dB SL compared to 15 dB SL. Better

483 thresholds at higher SLs are consistent with other AMD results (e.g., Stone &

484 Moore, 2014). In agreement with the FDLs, MDD thresholds were better for

485 listeners with music experience compared to those without. Importantly, there

486 was no interaction between music experience and noise exposure; therefore, the487 two effects can be discussed separately.

488 We found significantly better MDD thresholds for the High than for the Low Noise-Exposure group, but only at 25 dB SL. This was also observed in the 489 correlational analyses of the NESI score on the MDD thresholds, particularly at 490 491 6 kHz. These results do not support our hypothesis since they were in the opposite direction to that predicted. However, similar AMD results were 492 reported by Vinay & Moore, (2010) and an, albeit not significant trend, by 493 Prendergast et al. (2017b). Damage to OHCs is associated with a loss of cochlear 494 compression, which leads to abnormally rapid growth in loudness with level 495 (i.e., loudness recruitment) enhancing the perceived magnitude of envelope 496 fluctuations (Moore et al. 1996; Robles & Ruggero, 2001). This explanation is 497 498 not entirely convincing in the case of the present results, because of the lack of a frequency effect on the MDD thresholds: participants had similar MDD 499 thresholds at low frequency, with hearing in the normal range, and at high 500 frequency with mild or moderate hearing loss, hence presumably with some 501 502 OHC loss. Indeed, the rate of growth of loudness at low levels (near threshold) is similar in normal and impaired ears (Moore & Glasberg, 2004; Plack & Skeels, 503 2007). Furthermore, in tasks performed at 4 kHz and at 30 dB SL, participants 504 with moderate hearing loss (between 40 and 60 dB HL at 4 kHz) showed better 505 AMD but worse MDD thresholds than normal-hearing participants 506 (Schlittenlacher & Moore, 2016). The poor MDD in participants with hearing 507 loss has been associated with a saturation of fluctuation strength (Fastl, 1983). 508 However, this was observed only up to a modulation rate of 4 Hz (Fastl, 1983), 509

510 well below that of the 15 Hz used here. Recently, Wiinberg et al. (2019) measured AMD and MDD thresholds at 1 kHz at suprathreshold levels, both in 511 512 adults with normal hearing, and also those with mild to moderately severe sensorineural hearing loss. The latter had a similar AMD but worse MDD 513 thresholds than normal-hearing participants. The MDD results were interpreted 514 through the stochastic undersampling principle (Lopez-Poveda & Barrios, 2013, 515 but see also Marmel et al. 2015) as reduced fidelity in envelope encoding due to 516 a loss of IHCs. In contrast to the participants recruited by Schlittenlacher & 517 Moore (2016) and Wiinberg et al. (2019), we measured MDD in participants 518 519 with normal hearing thresholds up to 1 kHz, and mild-to-moderate hearing loss above 2 kHz. 520

521 Stone & Moore (2014) found that normal-hearing participants frequently

522 exposed to high-noise events (> 100 dBA SPL) had poorer AMD at 10 dB SL

523 compared to low noise-exposed control participants. On the other hand, older

524 participants showed better AMD at 10 dB SL than did their younger

525 participants. The different time scale of noise exposure of the participants may

526 lead to a combination of IHC and OHC dysfunction. In the current study, since

527 the MDD threshold varied with noise exposure, in particular at 25 dB SL and 6

528 kHz, irrespective of age and hearing threshold, the MDD threshold may be

529 associated only with OHC dysfunction.

530 **Conclusions**

In summary, no effect of noise exposure on FDLs was observed but they were
affected primarily by participants' music experience and age. MDD thresholds
improved with both music experience and noise exposure, with High Noise-

Exposed participants having lower thresholds. The results do not provide
evidence for a deficit related to IHC dysfunction; hence we hypothesize that they
could be related to OHC dysfunction. However, further research is required to
determine if hair cell pathway dysfunction underlies lower MDD thresholds,
and, if so, if there are differences in the relative contributions of IHC and OHC
dysfunction.

540 Acknowledgments

541 This work was supported by the NIHR Manchester Biomedical Research Centre

and by the Medical Research Council, UK (MR/L003589/1 and

543 MR/M023486/1). We are thankful to the participants for their patience and

544 cooperation. We thank Warren Bakay, Melanie Lough, Helen Massey and Helen

545 Whiston for their help with various aspects of this work. We also thank Garreth

546 Prendergast for helpful comments on a previous version of the manuscript.

547 Preliminary results of some of this work were presented at the International

548 Hearing Loss Conference (Niagara-on-the-Lake, Ontario, Canada, May 2019)

549 and e-Forum Acusticum (December 2020).

550 **References**

Allen, M., Poggiali, D., Whitaker, K., Marshall, T.R., Kievit, R.A., 2019.

- 552 Raincloud plots: a multi-platform tool for robust data visualization.
- 553 Wellcome Open Res 4, 63.
- 554 https://doi.org/10.12688/wellcomeopenres.15191.1
- 555 Baayen, R.H., Davidson, D.J., Bates, D.M., 2008. Mixed-effects modeling with 556 crossed random effects for subjects and items. Journal of Memory and
- 557 Language, Special Issue: Emerging Data Analysis 59, 390–412.
- 558 https://doi.org/10.1016/j.jml.2007.12.005
- Bates, D., Mächler, M., Bolker, B., Walker, S., 2015. Fitting Linear Mixed-Effects
 Models Using lme4. Journal of Statistical Software 67, 1–48.
- 561 https://doi.org/10.18637/jss.v067.i01
- 562 Bharadwaj, H.M., Masud, S., Mehraei, G., Verhulst, S., Shinn-Cunningham,
- 563 B.G., 2015. Individual differences reveal correlates of hidden hearing
 564 deficits. J. Neurosci. 35, 2161–2172.
- 565 https://doi.org/10.1523/JNEUROSCI.3915-14.2015
- 566 Bianchi, F., Carney, L.H., Dau, T., Santurette, S., 2019. Effects of Musical
- 567 Training and Hearing Loss on Fundamental Frequency Discrimination
- and Temporal Fine Structure Processing: Psychophysics and Modeling. J.
- 569
 Assoc. Res. Otolaryngol. 20, 263–277. https://doi.org/10.1007/s10162

 570
 018-00710-2
- 571 Bramhall, N., Beach, E.F., Epp, B., Le Prell, C.G., Lopez-Poveda, E.A., Plack,
- 572 C.J., Schaette, R., Verhulst, S., Canlon, B., 2019. The search for noise-
- induced cochlear synaptopathy in humans: Mission impossible? Hear.

574	Res. 377, 88–103. https://doi.org/10.1016/j.heares.2019.02.016
575	Bramhall, N.F., Konrad-Martin, D., McMillan, G.P., Griest, S.E., 2017. Auditory
576	Brainstem Response Altered in Humans With Noise Exposure Despite
577	Normal Outer Hair Cell Function. Ear Hear 38, e1–e12.
578	https://doi.org/10.1097/AUD.000000000000370
579	British Society of Audiology, 2018. Recommended Procedure: Pure-tone air-
580	conduction and bone-conduction threshold audiometry with and without
581	masking.
582	Burnham, K.P., Anderson, D.R., 2002. Model Selection and Multimodel
583	Inference: A Practical Information-Theoretic Approach, 2nd ed.
584	Springer-Verlag, New York. https://doi.org/10.1007/b97636
585	Carcagno, S., Plack, C.J., 2020. Effects of age on electrophysiological measures
586	of cochlear synaptopathy in humans. Hear Res 396, 108068.
587	https://doi.org/10.1016/j.heares.2020.108068
588	Chin, T., Rickard, N.S., 2012. The Music USE (MUSE) Questionnaire: An
589	Instrument to Measure Engagement in Music. MUSIC PERCEPT 29,
590	429–446. https://doi.org/10.1525/mp.2012.29.4.429
591	Couth, S., Prendergast, G., Guest, H., Munro, K.J., Moore, D.R., Plack, C.J.,
592	Ginsborg, J., Dawes, P., 2020. Investigating the effects of noise exposure
593	on self-report, behavioral and electrophysiological indices of hearing
594	damage in musicians with normal audiometric thresholds. Hear. Res.
595	108021. https://doi.org/10.1016/j.heares.2020.108021
596	Encina-Llamas, G., Harte, J.M., Dau, T., Shinn-Cunningham, B., Epp, B., 2019.
597	Investigating the Effect of Cochlear Synaptopathy on Envelope Following
598	Responses Using a Model of the Auditory Nerve. J. Assoc. Res.

599	Otolaryngol. https://doi.org/10.1007/s10162-019-00721-7
600	Ewert, D.E., 2013. AFC - A modular framework for running psychoacoustic
601	experiments and computational perception models. Proceedings of the
602	International Conference on Acoustics AIA-DAGA 1326–1329.
603	Ewert, S.D., Dau, T., 2004. External and internal limitations in amplitude-
604	modulation processing. J. Acoust. Soc. Am. 116, 478–490.
605	Fastl, H., 1983. Fluctuation Strength of Modulated Tones and Broadband Noise,
606	in: Klinke, R., Hartmann, R. (Eds.), HEARING — Physiological Bases and
607	Psychophysics. Springer, Berlin, Heidelberg, pp. 282–288.
608	https://doi.org/10.1007/978-3-642-69257-4_41
609	Furman, A.C., Kujawa, S.G., Liberman, M.C., 2013. Noise-induced cochlear
610	neuropathy is selective for fibers with low spontaneous rates. J.
611	Neurophysiol. 110, 577–586. https://doi.org/10.1152/jn.00164.2013
612	Grinn, S.K., Wiseman, K.B., Baker, J.A., Le Prell, C.G., 2017. Hidden Hearing
613	Loss? No Effect of Common Recreational Noise Exposure on Cochlear
614	Nerve Response Amplitude in Humans. Front Neurosci 11, 465.
615	https://doi.org/10.3389/fnins.2017.00465
616	Grose, J.H., Buss, E., Elmore, H., 2019. Age-Related Changes in the Auditory
617	Brainstem Response and Suprathreshold Processing of Temporal and
618	Spectral Modulation. Trends Hear 23, 2331216519839615.
619	https://doi.org/10.1177/2331216519839615
620	Grose, J.H., Buss, E., Hall, J.W., 2017. Loud Music Exposure and Cochlear
621	Synaptopathy in Young Adults: Isolated Auditory Brainstem Response
622	Effects but No Perceptual Consequences. Trends Hear 21,
623	2331216517737417. https://doi.org/10.1177/2331216517737417

624	Guest, H., Dewey, R.S., Plack, C.J., Couth, S., Prendergast, G., Bakay, W., Hall,
625	D.A., 2018. The Noise Exposure Structured Interview (NESI): An
626	Instrument for the Comprehensive Estimation of Lifetime Noise
627	Exposure. Trends Hear 22, 2331216518803213.
628	https://doi.org/10.1177/2331216518803213
629	Guest, H., Munro, K.J., Prendergast, G., Howe, S., Plack, C.J., 2017. Tinnitus
630	with a normal audiogram: Relation to noise exposure but no evidence for
631	cochlear synaptopathy. Hear. Res. 344, 265–274.
632	https://doi.org/10.1016/j.heares.2016.12.002
633	Hedge, C., Powell, G., Sumner, P., 2018. The reliability paradox: Why robust
634	cognitive tasks do not produce reliable individual differences. Behavior
635	Research Methods 50, 1166–1186. https://doi.org/10.3758/s13428-017-
636	0935-1
637	Heinrich, A., Knight, S., 2020. Reproducibility in Cognitive Hearing Research:
638	Theoretical Considerations and Their Practical Application in Multi-Lab
639	Studies. Front Psychol 11, 1590.
640	https://doi.org/10.3389/fpsyg.2020.01590
641	Johannesen, P.T., Pérez-González, P., Lopez-Poveda, E.A., 2014. Across-
642	frequency behavioral estimates of the contribution of inner and outer
643	hair cell dysfunction to individualized audiometric loss. Front Neurosci
644	8, 214. https://doi.org/10.3389/fnins.2014.00214
645	Johnson, P.C., 2014. Extension of Nakagawa & Schielzeth's R2GLMM to
646	random slopes models. Methods Ecol Evol 5, 944–946.
647	https://doi.org/10.1111/2041-210X.12225
648	Kishon-Rabin, L., Amir, O., Vexler, Y., Zaltz, Y., 2001. Pitch discrimination: are

649	professional musicians better than non-musicians? J Basic Clin Physiol
650	Pharmacol 12, 125–143. https://doi.org/10.1515/jbcpp.2001.12.2.125
651	Kobel, M., Le Prell, C.G., Liu, J., Hawks, J.W., Bao, J., 2017. Noise-induced
652	cochlear synaptopathy: Past findings and future studies. Hear. Res. 349,
653	148–154. https://doi.org/10.1016/j.heares.2016.12.008
654	Kujawa, S.G., Liberman, M.C., 2009. Adding insult to injury: cochlear nerve
655	degeneration after "temporary" noise-induced hearing loss. J. Neurosci.
656	29, 14077–14085. https://doi.org/10.1523/JNEUROSCI.2845-09.2009
657	Kumar, P., Upadhyay, P., Kumar, A., Kumar, S., Singh, G.B., 2017. Extended
658	high frequency audiometry in users of personal listening devices. Am J
659	Otolaryngol 38, 163–167. https://doi.org/10.1016/j.amjoto.2016.12.002
660	Kuznetsova, A., Brockhoff, P.B., Christensen, R.H.B., 2017. lmerTest Package:
661	Tests in Linear Mixed Effects Models. Journal of Statistical Software 82,
662	1–26. https://doi.org/10.18637/jss.v082.i13
663	Kuznetsova, A., Christensen, R.H.B., Bavay, C., Brockhoff, P.B., 2015.
664	Automated mixed ANOVA modeling of sensory and consumer data. Food
665	Quality and Preference 40, 31–38.
666	https://doi.org/10.1016/j.foodqual.2014.08.004
667	Le Prell, C.G., 2019. Effects of noise exposure on auditory brainstem response
668	and speech-in-noise tasks: a review of the literature. International
669	Journal of Audiology 58, S3–S32.
670	https://doi.org/10.1080/14992027.2018.1534010
671	Le Prell, C.G., Spankovich, C., Lobariñas, E., Griffiths, S.K., 2013. Extended
672	high-frequency thresholds in college students: effects of music player use
673	and other recreational noise. Journal of the American Academy of

674	Audiology 24, 725–739. https://doi.org/10.3766/jaaa.24.8.9
675	Lee, J., 1994. Amplitude modulation rate discrimination with sinusoidal
676	carriers. J. Acoust. Soc. Am. 96, 2140–2147.
677	Lenth, R., 2020. emmeans: Estimated Marginal Means, aka Least-Squares
678	Means.
679	Liberman, M.C., Epstein, M.J., Cleveland, S.S., Wang, H., Maison, S.F., 2016.
680	Toward a Differential Diagnosis of Hidden Hearing Loss in Humans.
681	PLoS ONE 11, e0162726. https://doi.org/10.1371/journal.pone.0162726
682	Liberman, M.C., Kujawa, S.G., 2017. Cochlear synaptopathy in acquired
683	sensorineural hearing loss: Manifestations and mechanisms. Hearing
684	Research 349, 138–147. https://doi.org/10.1016/j.heares.2017.01.003
685	Lopez-Poveda, E.A., Barrios, P., 2013. Perception of stochastically
686	undersampled sound waveforms: a model of auditory deafferentation.
687	Frontiers in Neuroscience 7, 124.
688	https://doi.org/10.3389/fnins.2013.00124
689	Lüdecke, D., Makowski, D., Waggoner, P., Indrajeet, P., 2020. performance:
690	Assessment of Regression Models Performance.
691	Lutman, M.E., Coles, R.R.A., Buffin, J.T., 2016. Guidelines for quantification of
692	noise-induced hearing loss in a medicolegal context. Clin Otolaryngol 41,
693	347–357. https://doi.org/10.1111/coa.12569
694	Marmel, F., Cortese, D., Kluk, K., 2020. The ongoing search for cochlear
695	synaptopathy in humans: Masked thresholds for brief tones in Threshold
696	Equalizing Noise. Hearing Research 107960.
697	https://doi.org/10.1016/j.heares.2020.107960
698	Marmel, F., Rodríguez-Mendoza, M.A., Lopez-Poveda, E.A., 2015. Stochastic

699	undersampling steepens auditory threshold/duration functions:
700	implications for understanding auditory deafferentation and aging. Front
701	Aging Neurosci 7, 63. https://doi.org/10.3389/fnagi.2015.00063
702	Micheyl, C., Delhommeau, K., Perrot, X., Oxenham, A.J., 2006. Influence of
703	musical and psychoacoustical training on pitch discrimination. Hear.
704	Res. 219, 36–47. https://doi.org/10.1016/j.heares.2006.05.004
705	Micheyl, C., Xiao, L., Oxenham, A.J., 2012. Characterizing the dependence of
706	pure-tone frequency difference limens on frequency, duration, and level.
707	Hear. Res. 292, 1–13. https://doi.org/10.1016/j.heares.2012.07.004
708	Moore, B.C., Peters, R.W., 1992. Pitch discrimination and phase sensitivity in
709	young and elderly subjects and its relationship to frequency selectivity. J
710	Acoust Soc Am 91, 2881–2893. https://doi.org/10.1121/1.402925
711	Moore, B.C.J., Glasberg, B.R., 2004. A revised model of loudness perception
712	applied to cochlear hearing loss. Hearing Research 188, 70–88.
713	https://doi.org/10.1016/S0378-5955(03)00347-2
714	Moore, B.C.J., Glasberg, B.R., Stone, M.A., 2004. New version of the TEN test
715	with calibrations in dB HL. Ear Hear 25, 478–487.
716	Moore, B.C.J., Wojtczak, M., Vickers, D.A., 1996. Effect of loudness recruitment
717	on the perception of amplitude modulation. The Journal of the Acoustical
718	Society of America 100, 481–489. https://doi.org/10.1121/1.415861
719	Nakagawa, S., Johnson, P.C.D., Schielzeth, H., 2017. The coefficient of
720	determination R2 and intra-class correlation coefficient from generalized
721	linear mixed-effects models revisited and expanded. J R Soc Interface 14.
722	https://doi.org/10.1098/rsif.2017.0213
723	Nakagawa, S., Schielzeth, H., 2013. A general and simple method for obtaining

724	R2 from generalized linear mixed-effects models. Methods in Ecology
725	and Evolution 4, 133–142. https://doi.org/10.1111/j.2041-
726	210x.2012.00261.x
727	Oxenham, A.J., 2016. Predicting the Perceptual Consequences of Hidden
728	Hearing Loss. Trends Hear 20, 2331216516686768.
729	https://doi.org/10.1177/2331216516686768
730	Plack, C.J., Léger, A., Prendergast, G., Kluk, K., Guest, H., Munro, K.J., 2016.
731	Toward a Diagnostic Test for Hidden Hearing Loss. Trends Hear 20.
732	https://doi.org/10.1177/2331216516657466
733	Plack, C.J., Skeels, V., 2007. Temporal integration and compression near
734	absolute threshold in normal and impaired ears. J. Acoust. Soc. Am. 122,
735	2236–2244. https://doi.org/10.1121/1.2769829
736	Prendergast, G., Couth, S., Millman, R.E., Guest, H., Kluk, K., Munro, K.J.,
737	Plack, C.J., 2019. Effects of Age and Noise Exposure on Proxy Measures
738	of Cochlear Synaptopathy. Trends Hear 23, 2331216519877301.
739	https://doi.org/10.1177/2331216519877301
740	Prendergast, G., Guest, H., Munro, K.J., Kluk, K., Léger, A., Hall, D.A., Heinz,
741	M.G., Plack, C.J., 2017a. Effects of noise exposure on young adults with
742	normal audiograms I: Electrophysiology. Hear. Res. 344, 68–81.
743	https://doi.org/10.1016/j.heares.2016.10.028
744	Prendergast, G., Millman, R.E., Guest, H., Munro, K.J., Kluk, K., Dewey, R.S.,
745	Hall, D.A., Heinz, M.G., Plack, C.J., 2017b. Effects of noise exposure on
746	young adults with normal audiograms II: Behavioral measures. Hear.
747	Res. 356, 74–86. https://doi.org/10.1016/j.heares.2017.10.007
748	Pumplin, J., 1985. Low-noise noise. J. Acoust. Soc. Am. 78, 100–104.

749	https://doi.org/10.1121/1.392571
750	R Core Team, 2020. R: A Language and Environment for Statistical Computing.
751	R Foundation for Statistical Computing, Vienna, Austria.
752	Robles, L., Ruggero, M.A., 2001. Mechanics of the mammalian cochlea. Physiol.
753	Rev. 81, 1305–1352. https://doi.org/10.1152/physrev.2001.81.3.1305
754	Schaette, R., McAlpine, D., 2011. Tinnitus with a normal audiogram:
755	physiological evidence for hidden hearing loss and computational model.
756	J. Neurosci. 31, 13452–13457.
757	https://doi.org/10.1523/JNEUROSCI.2156-11.2011
758	Schlittenlacher, J., Moore, B.C.J., 2016. Discrimination of amplitude-
759	modulation depth by subjects with normal and impaired hearing. J.
760	Acoust. Soc. Am. 140, 3487. https://doi.org/10.1121/1.4966117
761	Sergeyenko, Y., Lall, K., Liberman, M.C., Kujawa, S.G., 2013. Age-related
762	cochlear synaptopathy: an early-onset contributor to auditory functional
763	decline. J. Neurosci. 33, 13686–13694.
764	https://doi.org/10.1523/JNEUROSCI.1783-13.2013
765	Shehorn, J., Strelcyk, O., Zahorik, P., 2020. Associations between speech
766	recognition at high levels, the middle ear muscle reflex and noise
767	exposure in individuals with normal audiograms. Hear. Res. 392,
768	107982. https://doi.org/10.1016/j.heares.2020.107982
769	Smoorenburg, G.F., 1992. Speech reception in quiet and in noisy conditions by
770	individuals with noise-induced hearing loss in relation to their tone
771	audiogram. J. Acoust. Soc. Am. 91, 421–437.
772	https://doi.org/10.1121/1.402729
773	Stellmack, M.A., Viemeister, N.F., Byrne, A.J., 2006. Discrimination of depth of

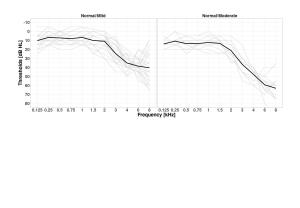
sinussidal amplituda madulation with and without neved corrigations.
sinusoidal amplitude modulation with and without roved carrier levels. J.
Acoust. Soc. Am. 119, 37–40. https://doi.org/10.1121/1.2133576
Stone, M.A., Moore, B.C.J., 2014. Amplitude-modulation detection by
recreational-noise-exposed humans with near-normal hearing thresholds
and its medium-term progression. Hear. Res. 317, 50–62.
Stone, M.A., Moore, B.C.J., Greenish, H., 2008. Discrimination of envelope
statistics reveals evidence of sub-clinical hearing damage in a noise-
exposed population with "normal" hearing thresholds. Int J Audiol 47,
737–750. https://doi.org/10.1080/14992020802290543
Sulaiman, A.H., Husain, R., Seluakumaran, K., 2014. Evaluation of early
hearing damage in personal listening device users using extended high-
frequency audiometry and otoacoustic emissions. Eur Arch
Otorhinolaryngol 271, 1463–1470. https://doi.org/10.1007/s00405-013-
2612-z
Valderrama, J.T., Beach, E.F., Yeend, I., Sharma, M., Van Dun, B., Dillon, H.,
2018. Effects of lifetime noise exposure on the middle-age human
auditory brainstem response, tinnitus and speech-in-noise intelligibility.
Hear. Res. 365, 36–48. https://doi.org/10.1016/j.heares.2018.06.003
Valero, M.D., Burton, J.A., Hauser, S.N., Hackett, T.A., Ramachandran, R.,
Liberman, M.C., 2017. Noise-induced cochlear synaptopathy in rhesus
monkeys (Macaca mulatta). Hear Res 353, 213–223.
https://doi.org/10.1016/j.heares.2017.07.003
Verhulst, S., Ernst, F., Garrett, M., Vasilkov, V., 2018. Suprathreshold
Psychoacoustics and Envelope-Following Response Relations: Normal-
Hearing, Synaptopathy and Cochlear Gain Loss. Acta Acustica united

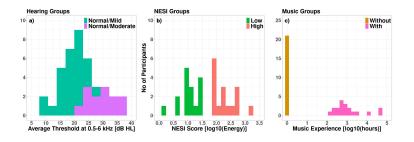
799	with Acustica 104, 800–803. http://dx.doi.org/10.3813/aaa.919227
800	Vinay, S.N., Moore, B.C.J., 2010. Effects of the use of personal music players on
801	amplitude modulation detection and frequency discrimination. J. Acoust.
802	Soc. Am. 128, 3634–3641. https://doi.org/10.1121/1.3500679
803	Wakefield, G.H., Viemeister, N.F., 1990. Discrimination of modulation depth of
804	sinusoidal amplitude modulation (SAM) noise. J. Acoust. Soc. Am. 88,
805	1367–1373.
806	Wickham, H., 2009. ggplot2: Elegant Graphics for Data Analysis, Use R!
807	Springer-Verlag, New York. https://doi.org/10.1007/978-0-387-98141-3
808	Wiinberg, A., Jepsen, M.L., Epp, B., Dau, T., 2019. Effects of Hearing Loss and
809	Fast-Acting Compression on Amplitude Modulation Perception and
810	Speech Intelligibility. Ear and Hearing 40, 45–54.
811	https://doi.org/10.1097/AUD.000000000000589
812	Winter, B., 2013. Linear models and linear mixed effects models in R with
813	linguistic applications. arXiv:1308.5499 [cs].
814	Yeend, I., Beach, E.F., Sharma, M., Dillon, H., 2017. The effects of noise
815	exposure and musical training on suprathreshold auditory processing
816	and speech perception in noise. Hear. Res. 353, 224–236.
817	https://doi.org/10.1016/j.heares.2017.07.006
818	

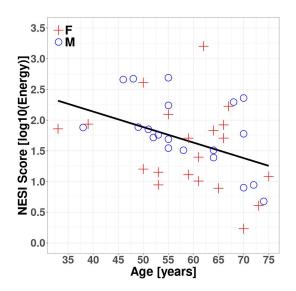
819 Figures Legends

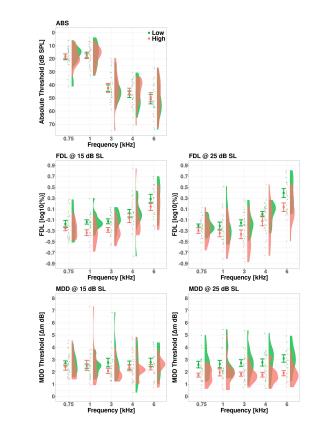
821	Figure 1: Test-ear mean pure tone thresholds (black) and test-ear pure tone
822	thresholds for each of the 40 participants (gray) in the Normal/Mild haring
823	group (left panel) and Normal/Moderate hearing group (right panel).
824	
825	Figure 2: Distributions of average pure tone hearing thresholds at 0.5, 0.75, 1,
826	3, 4 and 6 kHz (panel a), noise exposure structured interview (NESI) score
827	(panel b), and music experience (panel c).
828	
829	Figure 3: Noise exposure scores as a function of age for the 40 participants.
830	
831	Figure 4: Mean data with SEs, individual data, and probability densities of
832	ABS, FDL and MDD thresholds for the Low and High Noise-exposure groups.
833	
834	Figure 5: Interaction between Noise Exposure (Low vs High) and Music
835	Experience (Without vs With) groups in the MDD task at 25 SL dB averaged
836	over frequency.
837	
838	Figure S1: Mean with SE, individual data and probability densities of ABS,
839	FDL and MDD thresholds for the Hearing groups.

- **Figure S2**: Mean with SE, individual data and probability densities of ABS,
- 842 FDL and MDD thresholds for the Music groups.
- **Figure S3**: FDLs as a function of age at 0.75 kHz (r = 0.123, *p* = 0.284), 1 kHz
- 845 (r = 0.227, p = 0.045), 3 kHz (r = 0.260, p = 0.020), 4 kHz (r = 0.257, p =
- 846 0.023) and 6 kHz (r = 0.381, p = 0.001) averaged over SL.









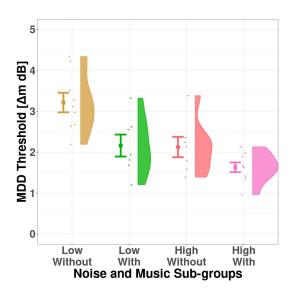


Table 1: Spearman's rho coefficients for the relation between psychophysical (ABS, MDD, and FDL) tasks and lifetime noise exposure (NESI); partial Spearman correlation between psychophysical tasks and lifetime noise exposure controlling separately for each of music experience, Age and ABS; and Age. Positive correlations indicate worse performance with increasing noise exposure or age. Negative correlations indicate better performance with increasing music experience or age. Key: * = p ≤ 0.05; ** = p ≤ 0.01; *** = p ≤ 0.001 (uncorrected).

Task	Frequency [kHz]						
NEGT	0.75	1	3	4	6		
NESI							
FDL 15	-0.08	-0.34*	-0.36*	-0.27	-0.24		
FDL 25	-0.22	-0.04	-0.26	-0.17	-0.41*		
MDD 15	-0.20	0.01	-0.31	-0.13	-0.30		
MDD 25	-0.42**	-0.31	-0.45**	-0.44**	-0.59***		
NESI, controlling for Age							
FDL 15	-0.04	-0.28	-0.26	-0.21	-0.12		
FDL 25	-0.17	0.09	-0.18	-0.04	-0.31		
MDD 15	-0.16	-0.07	-0.23	-0.17	-0.2		
MDD 25	-0.39*	-0.37*	-0.40*	-0.41**	-0.54**		
NESI, controlling for Music							
FDL 15	0.09	-0.25	-0.29	-0.18	-0.12		
FDL 25	-0.11	0.08	-0.19	-0.10	-0.37*		
MDD 15	-0.04	0.08	-0.24	-0.06	-0.18		
MDD 25	-0.33*	-0.14	-0.44**	-0.38*	-0.52**		
NESI, co	ontrolling	g for ABS	5				
FDL 15	-0.07	-0.35*	-0.38*	-0.26	-0.23		
FDL 25	-0.22	-0.04	-0.26	-0.16	-0.42*		
MDD 15	-0.19	0.01	-0.31	-0.12	-0.29		
MDD 25	-0.41*	-0.31	-0.45**	-0.44**	-0.59***		
Age							
FDL 15	0.09	0.20	0.32*	0.19	0.34*		
FDL 25	0.17	0.28	0.22	0.31	0.42^{*}		
MDD 15	0.13	-0.15	0.24	-0.04	0.33		
MDD 25	0.15	-0.06	0.21	0.16	0.30		

