



1 Article

# 2 Dairy-inspired coatings for bone implants from whey 3 protein isolate-derived self-assembled fibrils

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16 **Abstract:** To improve integration of a biomaterial with surrounding tissue, its surface properties  
17 may be modified by adsorption of biomacromolecules, e.g. fibrils. Whey protein isolate (WPI), a  
18 dairy industry by-product, supports osteoblastic cell growth. WPI's main component,  $\beta$ -  
19 lactoglobulin, forms fibrils in acidic solutions. In this study, aiming to develop coatings for  
20 biomaterials for bone contact, substrates were coated with WPI fibrils obtained at pH 2 or 3.5.  
21 Importantly, WPI fibrils coatings withstood autoclave sterilization and appeared to promote human  
22 bone marrow stromal cells (hBMSC) spreading and differentiation. In the future, WPI fibrils  
23 coatings could facilitate immobilization of biomolecules with growth stimulating or antimicrobial  
24 properties.

25 **Keywords:** coating, stem cell, whey protein isolate, bone, fibril

## 27 1. Introduction

28 Whey protein isolate (WPI) is a dairy industry by-product which contains > 95% protein, of  
29 which 75% is  $\beta$ -lactoglobulin [1]. Previous studies showed that WPI enhances cell proliferation and  
30 osteogenic differentiation and displays antibacterial properties [1–3]. Upon heating under acidic  
31 conditions,  $\beta$ -lactoglobulin degrades into smaller peptides which undergo self-assembly to form  
32 fibrils several micrometers long and a few nm thick [4], whose morphology is pH-dependent (long  
33 semi-flexible fibers at pH 2, worm-like structures at pH 3.5) [5–7].

34 Better cell-biomaterial interactions, and biomaterial integration into host tissue can be achieved  
35 by improving surface properties, e.g. by coatings. Fibrillar coatings have advantages including high  
36 surface/volume ratio, promoting fibril adhesion to substrates. Biologically active molecules can be  
37 immobilized on fibrils [8,9], which can form aligned superstructure scaffolds [10], improve cell line  
38 attachment and act as biomimetic cell culture platforms [11–13].

39 A commonly used fibrillar molecule used as implant coating materials is collagen, which is  
40 known to promote cell adhesion, spreading and proliferation [14–18]. Fibronectin is another  
41 commonly used molecule to improve cell adhesion, also in fibrillar form [19,20]. One advantage of  
42 WPI is its low cost, as it is a by-product of the dairy industry.

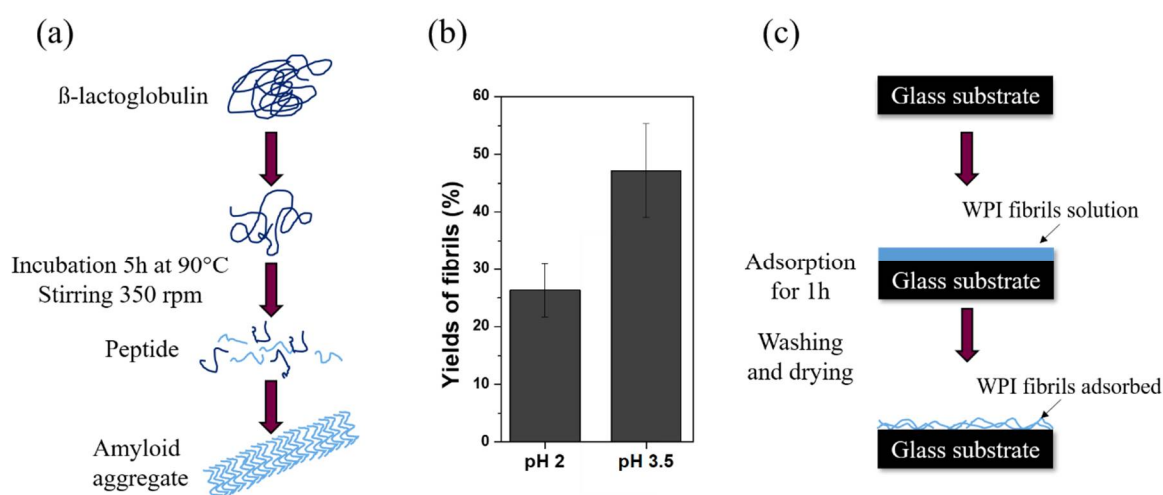
43 With the intention of developing coatings for biomaterials for bone contact, WPI fibrillar  
44 coatings were formed to support and enhance spreading, attachment and differentiation of hBMSC,  
45 which have greater clinical relevance than cell lines. WPI fibrils were hypothesized to withstand

46 autoclaving as WPI hydrogels do [21]. Autoclaving was preferred due to its ubiquity, clinical  
47 acceptance and low cost.

48 WPI fibrils were formed in solutions at two different pH values, 2 and 3.5. A WPI solution  
49 concentration of 2.5 wt% was used. WPI concentrations between 2.5 % and 5 % WPI were found to  
50 result in a high fibril yield [3,4], and especially 2.5 % WPI is often used in WPI or beta-Lactoglobulin  
51 fibril studies due to the lower sample viscosity which improves handling. Because the protein  
52 concentration also affects the aggregation kinetics and morphology of the resulting aggregates [22–  
53 24], deviations from these ideal values can also reduce the comparability to other studies. and then  
54 adsorbed onto substrates and imaged by Scanning Electron Microscopy (SEM). Finally, autoclaved  
55 coatings were characterized using hBMSC.  
56

## 57 2. Results and discussion

58 WPI fibril formation (shown schematically in Figure 1a) was influenced by pH, as measurements  
59 of fibrillar yield at pH 2 (approximately 25%) and pH 3.5 (> 40%) demonstrated (Figure 1b). Similar  
60 observations were reported previously [5–7]. Differences in yield are attributed to differences in the  
61 fibril building blocks, which are specific acid hydrolysed peptides at pH 2 [4], but unspecific non-  
62 hydrolyzed proteins at pH 3.5 [5].  
63



64

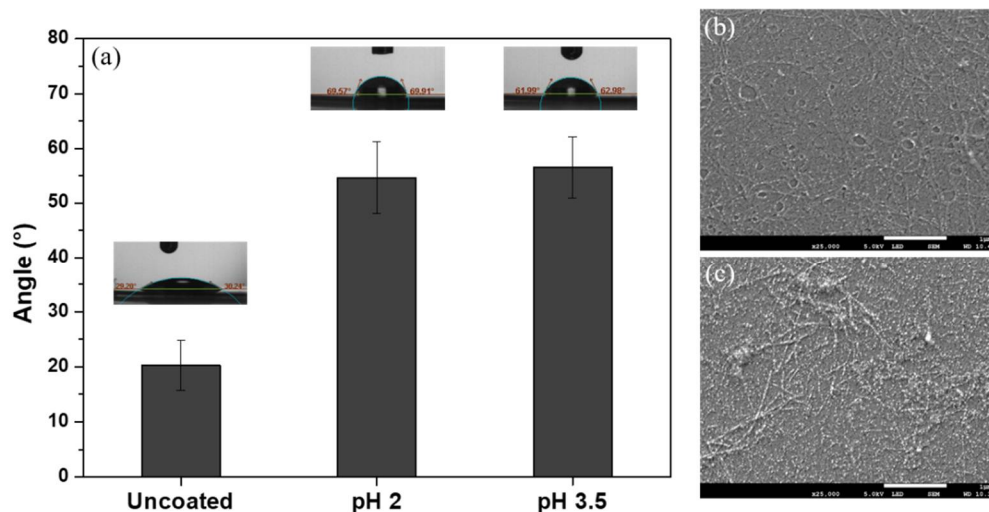
65 **Figure 1.** (a) Process of fibrils formation at pH 2 in solution; at pH 2,  $\beta$ -lactoglobulin denatures and  
66 hydrolyses at 90°C. Specific peptides self-associate into the amyloid aggregates, which can consist of  
67 approximately three intertwined protofibrils. At pH 3.5, acid hydrolysis is reduced; therefore non-  
68 hydrolyzed  $\beta$ -lactoglobulin assembles into worm-like aggregates, which are not amyloid but  
69 amyloid-like and of different shape and morphology than at pH. (b) Fibrillar yield in solutions of  
70 different pH and (c) adsorption of WPI fibrils on glass substrates.

71

72 Contact angle (CA) measurements demonstrated a significant increase from 20 to approximately  
73 55° on both coated sample types (Figure 2a). Similar increases were reported for edible WPI fibril  
74 coatings on fruits [25]. Advantageously for cell growth, CA remains lower than 100° [26]. A  
75 hydrophilic surface is beneficial for cell adhesion to make sure that proteins from cell culture medium  
76 adsorb to the surface in the desired conformation, so that binding sites on the proteins are recognized  
77 by the cells. Furthermore, a lower contact angle and higher wettability would facilitate coating of  
78 rough or porous biomaterial surfaces.

79 SEM images confirmed that fibril coatings withstood washing and drying. Fibrils prepared at  
80 pH 3.5 (Figure 2c) appeared to be shorter and less straight than those formed at pH 2 (Figure 2b), in  
81 agreement with previous studies [5]. Fibrils were detected by SEM after autoclaving (supplementary

82 information, figure S1); hence, they withstand sterilization. Adhesion of the fibrils to substrates  
83 would hinder fibril aggregation and degradation as in previous studies [27,28]; hence the coating is  
84 estimated to be one fibril thick.



85

86 **Figure 2.** (a) CA measurements of uncoated and fibrillar coated samples with solution at pH 2 and  
87 pH 3.5 and SEM images of fibrillar coatings obtained at (b) pH 2 and (c) pH 3.5 (scale bar: 1 μm)

88

89 Adhesion of hBMSC was confirmed on the uncoated (Figure 3a) and coated samples  
90 (Figure 3b,c). Spreading was superior and tissue non-specific alkaline phosphatase (TNAP) activity  
91 (a marker of osteogenic differentiation and linked to the calcium deposition as shown previously  
92 [9,29]) was higher on coated samples (Figure 3g). The cells became confluent over the WPI coatings.

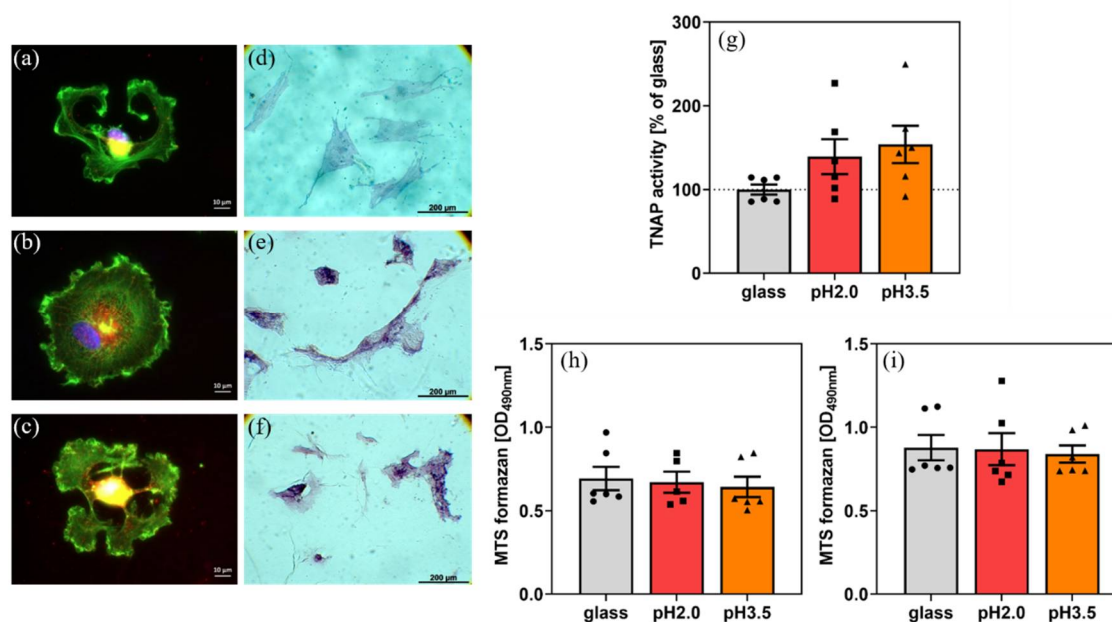
93 hBMSC on coated samples showed 2 h after seeding clear focal adhesion contacts and a well-  
94 organized cytoskeleton. A possible reason for that could be that diverse proteins from the serum and  
95 cellular in situ-formed proteins adsorbed on the WPI layer and thus promoted initial adhesion. The  
96 cell number on coated samples at day 2 and day 4 after seeding (MTS formazan formation is a  
97 measure of cell number and can be used as an index of cell proliferation) did not differ substantially  
98 from that on glass.

99 For hBMSC, proper adhesion, spreading and re-organization of cytoskeleton is an essential  
100 prerequisite for proliferation and differentiation of the cells. The fibrillar coating promoted the  
101 adhesion and re-organization of the cytoskeleton of hBMSC, did not influence the number of  
102 adherent cells, but obviously improved their “quality” as evidenced by higher TNAP activity.

103 Hence, we suspect that the coatings induced a superior start of the differentiation program of  
104 cells. Analysis concerning the molecular mechanisms are planned for future studies. In the present  
105 study, we wished to ascertain whether such a fibrillar coating has advantages for hBMSC adhesion  
106 and promotes osteogenic parameters.

107 Apparently differences in yields and morphologies of straight fibrils observed at pH 2 and the  
108 worm-like aggregates observed at pH 3.5 do not affect hBMSC. hBMSC metabolic activity increased  
109 slightly from day 2 to 4 (Figure 3h,i), but not significantly.

110



111

112 **Figure 3.** (a) Morphology of hBMSC on (a) glass, (b) fibrillar coating (pH=2), (c) fibrillar coating  
 113 (pH=3.5), 2 h after plating, and (d), (e), (f) TNAP staining at day 11 after plating, respectively. (g)  
 114 TNAP activity on different substrates (day 11) and metabolic activity results at (h) day 2 and (i) day  
 115 4 after plating.

116 Future work will focus on preparation of coatings from fibrils obtained at other pH values. It is  
 117 well known that the typical fibrils with amyloid structure only occur at pH 2, while worm-like  
 118 aggregates can be observed at pH 3.5 [6]. Spherical aggregates emerge at pH 4 to 5 [7] and otherwise  
 119 there are also smaller aggregates observed at neutral pH. Besides pH-induced changes, the addition  
 120 of sodium chloride or the protein concentration can affect the morphology, as well as addition of  
 121 solvents [22,30]. The structures have different yields (i.e., portion of amyloid to non-assembled  
 122 material) but also different processing stabilities. Thus, there is a whole range of conditions that can  
 123 be used to alter the morphology and to study the correlation between structure and cell behaviour in  
 124 the future.

125 Another focus of future work will be extension of the cell biological characterization of the  
 126 coatings to elucidate the exact mechanism by which coatings may promote differentiation and to  
 127 include cell-induced mineralization. From previous investigations, it is known that an increase of  
 128 TNAP activity leads to an increase in released phosphate ions into the conditioned medium and in  
 129 consequence to enhanced mineralization [9], which should be studied in future.

130 WPI fibrillar coatings can be enhanced by incorporation of molecules with growth-stimulatory  
 131 or antimicrobial properties into the coatings, coating thickness and mechanical measurements and  
 132 substrates more appropriate for bone contact (e.g. titanium alloy). Furthermore, WPI fibrillar coatings  
 133 should be compared to more commonly used fibrillar coatings of fibronectin and collagen, which are  
 134 known to promote cell adhesion [14–20].

135

#### 136 4. Materials and Methods

137 WPI (BiPro, Davisco Foods International Inc., USA) was dissolved in Milli-Q (2.5 wt%). pH was  
 138 set to 2 and 3.5 by adding HCl. 15 mL WPI solution was heated (90°C, 5h, stirring speed 350 rpm) to  
 139 induce fibril formation resulting in a fibrillar suspension. Glass substrates (chosen as an inexpensive  
 140 substrate for this pilot study) were coated with fibrils by adsorption from the suspension. Substrates  
 141 were rinsed with Milli-Q to remove non-adhered fibrils, air-dried and autoclaved (121°C, 15  
 142 minutes). SEM, CA measurements and fibrillar yield quantification were performed as described  
 143 previously [5,7,31,32].

144 hBMSC were isolated from bone marrow aspirates from donors (males, average  $27 \pm 5$  yrs.) who  
145 gave full informed consent (local ethics commission (ethic vote No. EK466112016)), at the Bone  
146 Marrow Transplantation Center, University Hospital Dresden, characterized and plated onto  
147 samples ( $5,555$  hBMSC/cm<sup>2</sup>) as described previously [29,33].

148 After 2h, hBMSC morphology was monitored by fluorescence staining of F-actin and  
149 phosphorylated focal adhesion kinase, as described previously [8]. Metabolic activity of hBMSC was  
150 determined by the standard MTS assay (Cell Titer96 AQueous One Solution Proliferation Assay)  
151 (Promega, Mannheim, Germany). Cell culture medium was replaced by fresh medium containing  
152 10% of MTS dye solution. After incubation in a humidified CO<sub>2</sub> incubator (2h, 37°C), 80 µL medium  
153 was removed and absorbance was measured photometrically at 490 nm.

154 At day 11 after seeding hBMSC were stained for tissue non-specific alkaline phosphatase  
155 (TNAP) enzyme activity with a commercial staining kit (86-R, Sigma). Images were obtained and  
156 TNAP enzyme activity was determined, as described previously [8].

157 Experiments were performed with cells from three different donors (n=3) each in triplicate.  
158 Results are presented as mean  $\pm$  standard error of the mean. Statistical significance was analysed with  
159 GraphPad Prism 8.4 software (Statcon, Witzenhausen, Germany) by ANOVA analysis with  
160 Bonferroni's post-test.  
161

## 162 5. Conclusions

163 Formation of WPI fibrils in solution was strongly pH-dependant; fibrillar yield increased when  
164 pH was increased from 2 to 3.5. WPI fibrillar coatings resisted autoclave sterilization and supported  
165 the attachment, spreading and differentiation of hBMSC. The pH 2 and pH 3.5 fibrils had an equally  
166 positive effect on cell differentiation.

167 **Supplementary Materials:** Supplementary materials can be found at [www.mdpi.com/xxx/s1](http://www.mdpi.com/xxx/s1).

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169 formal analysis, R.R., U.H., J.A. and T.E.L.D.; investigation, R.R., U.H., J.A. and T.E.L.D.; resources, J.K.K., U.H.  
170 and T.E.L.D.; data curation, R.R., U.H. and J.A.; writing—original draft preparation, L.M., J.K.K. and T.E.L.D.;  
171 writing—review and editing, L.M. and T.E.L.D.; visualization, U.H., R.R. and T.E.L.D.; supervision, T.E.L.D. and  
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177 study; in the collection, analyses, or interpretation of data; in the writing of the manuscript, or in the decision to  
178 publish the results.

## 179 Abbreviations

|       |  |
|-------|--|
| CA    | Contact angle                            |
| hBMSC | Human bone marrow stromal cells          |
| SEM   | Scanning electron microscopy             |
| TNAP  | Tissue non-specific alkaline phosphatase |
| WPI   | Whey protein isolate                     |

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